

# **Patent Application**

Title Of The Invention

**METHOD FOR CURING CYANOACRYLATE ADHESIVES**

Inventor

Max Azevedo  
1979 Wild Briar Lane  
Lenoir, NC 28645  
Citizen of U.S.A.

099222-10191  
"OFFICE" 9222850

## BACKGROUND OF THE INVENTION

### 1. *Field of the Invention*

This invention relates broadly to a new method of curing stabilized cyanoacrylate adhesives coincidently with their application to a substrate, particularly with reference to medical procedures using such adhesives and new devices for using the method.

### 2. *Description of the Prior Art*

Medical interest in cyanoacrylate polymers was apparent in the mid-nineteen sixties as evidenced by numerous reports on its use as a tissue bonding agent. Collins, et al reported on the effectiveness of homologous chain cyanoacrylates for bonding of biological substrates (1,2). They observed high rates of polymerization with longer chain esters than the methyl or ethyl monomers. There appeared to be more biocompatibility with the longer chains as noted by the ease of spreading monomer films on biosubstrates. This contrasted with in vitro polymerizations where the lower homologues reacted much faster. There was particular interest in the degradation of these polymers as they related to possible harmful effects that would preclude their use in surgery. Woodward, et al (3) reported histotoxicity of these monomers in rat tissue. The study involved in situ polymerization of three cyanoacrylate monomers: methyl, hexyl, decyl. It was reported that histotoxic effects were greatest with methyl and decreased with the other two monomers.

The same group reported on the use of radioactive methyl cyanoacrylate for monitoring routes for the loss of the polymer (4, 5). Results indicated that the polymer was degraded and excreted principally through the urine and feces. Analysis of the animal's organs revealed no signs of radioactivity. This implied no degradation products were incorporated into any of the animal's metabolic pathway. By analogy to vinylidene cyanide, they noted that the cyanoacrylate polymer degraded in the presence of water and more so in the presence of bases. The first observed degradation product turned out to be one of the starting materials, i.e., formaldehyde. In vitro studies have shown that the polymers degrade via hydrolytic scission in homogeneous as well as heterogeneous conditions (6). These degradation products were confirmed to be formaldehyde and the corresponding cyanoacetate. The conditions of solution degradation affected the consequent rates, namely, under neutral conditions rates

1 decreased as the homologous series was ascended while alkaline conditions increased all  
2 rates.

3 The same study reported that the hydroxyl group was evident in the polymer as  
4 the initiating species. This was concluded from infrared spectral data that displayed  
5 hydroxyl group absorption at 3600  $\text{cm}^{-1}$ . Further support for this is the noted  
6 suppression of the OH as water is replaced with methanol and the observed methoxy  
7 absorption at 1100  $\text{cm}^{-1}$ . Preferential initiation was shown to occur with  $\text{NH}_2$   
8 containing substances such as pyridine, cysteine, alanine, and glycine in aqueous  
9 solutions. This suggested that in vivo adhesion was more than a mechanical interlocking  
10 of the solid polymer with the tissue. This appears to be the case as it was noted that  
11 typical polymer solvents were not effective in solvating tissue-bound polymer.

12 From this it would appear that in vivo studies of degradation do not necessarily  
13 correspond to in vitro conditions. Part of the degradation mechanism relies on the  
14 solution of polymer for hydrolytic scission. The chemical bonding of the polymer  
15 excludes this surface from hydrolytic activity. A mechanism of degradation was proposed  
16 that suggests an action similar to unzipping in acrylics, however, the difference being that  
17 the monomer is not regenerated. The proposed mechanism necessitates the presence of  
18 the hydroxyl as well as the presence of water.

19 An unusual effect was reported regarding the aqueous degradation of isobutyl  
20 cyanoacrylate (7). Of the monomers tested (methyl, propyl, butyl, isobutyl, heptyl ,  
21 octyl), it was the only one that degraded more rapidly than any of the unbranched  
22 homologues, with the exception of the methyl.

23 A second study reported that in vivo experimentation give credence to the chain  
24 scission mechanism by hydrolysis (8). When beta-(14) carbon tagged cyanoacrylate is  
25 implanted in rats, radioactive urea is isolated from urine. This suggests that tagged  
26 formaldehyde is released, converted to carbon dioxide and in turn reacts with ammonia to  
27 produce urea (9).

28 Rates of degradation on ethyl, butyl, and hexyl cyanoacrylates were evaluated  
29 with regards to molecular weights, concentrations, and side chain structures (10). The  
30 method employed buffered systems of pH ranges from 5.97 to 7.88. As expected, the  
31 rates increased with increasing pH. Scanning electron microscopy of the degraded  
32 polymer indicated that reaction occurs at the surfaces and not internally through

1 diffusion. It was postulated that the greater the length of the nalkyl side chain, the more  
2 protection provided to the labile hydroxyl end of the polymer chain. This in turn would  
3 provide greater resistance to degradation of the polymer. Degradation rates do in fact  
4 correspond to chain length protection. The relative rates of degradation for hexyl, butyl,  
5 and ethyl were, respectively, 1.0, 1.36, 9.55.

6 The same group reported on a study whereby degradation rates were retarded by  
7 increasing the chain length of the polymer (11). Very small quantities of impurities in the  
8 monomers had a significant impact on the final outcome of the degree of polymerization.  
9 Further to this study, within the ethoxyethyl system, longer chain length enhanced the  
10 degradation resistance of the resultant polymer.

11 A comparative study of ethyl cyanoacrylate and polyurethane in-situ generated  
12 adhesives and coatings were reported in US patent 4,057,535. The study claimed the  
13 superiority of the polyurethane structure due to high flexibility and compatibility with  
14 the treated tissues. The single comparison was made with incised tissue and  
15 consequent application between the wound edges. Inferiority of this application for  
16 the cyanoacrylate was readily evident, but true topical applications were not  
17 compared. Of eleven examples given, four were of a topical method, yet no data was  
18 presented as no application of the ethyl or any other homologue was done  
19 conjunctively for comparative efficacy. A further deficiency of this patent is the  
20 practicality of use. No indication is given for a device to properly apply the two part  
21 system and appears to indicate an at-site preparation.

22 Another patent, US 5,192,536 overcomes the apparent difficulty of 4,057,535  
23 by taking preformed polyurethane and dissolving in a rapidly evaporating solvent  
24 such as tetrahydrofuran. The composition is designed to form a "membrane-like cover  
25 over the wound" and "assists in maintaining closure of the wound". Again no  
26 comparative studies were reported.

27 US patent 3,995,641 presents the novelty of modified cyanoacrylates, namely,  
28 carbalkoxyalkyl cyanoacrylates. These also are claimed to be useful for tissue  
29 adhesives in surgical applications. The presumed superiority of these products was  
30 attributable to the rapid hydrolytic decay and concurrent low degree of histotoxicity.  
31 Since no data is presented regarding formaldehyde evolution it is presumed that the  
32 hydrolysis mechanism does not scission the polymer to generate it.

1 US patent 5,254,132 discloses the use of a hybrid method of surgical  
2 application of cyanoacrylates. It claims a combination of sutures and adhesive such as  
3 to be mutually isolated from each other, but to both support the re-growth of the  
4 tissue in the wound area. It addresses the issue of insuring no contact of adhesive in  
5 the suture area so as to assure no inclusions of the cyanoacrylate. This method would  
6 appear to be awkward and cumbersome and require a very effective and controlled  
7 dispensing of the adhesive without contacting the suture. Additional concern is  
8 indicated as a suggestion is made to employ a solvent (acetone) if any surgical  
9 instrument happens to be bonded inadvertently to the treated area.

10 US patent 5,328,687 attacks the formaldehyde issue by incorporating a  
11 formaldehyde scavenger such as sodium bisulfite. The various compositions were  
12 evaluated via in-vitro experimentation. The examples presented all had a presumably  
13 excessive level of scavenger. The representative compositions had loadings of 20% of  
14 a scavenging agent that was designed to offset formaldehyde emissions that were at  
15 0.1%. As indicated previously, in-vitro and in vivo conditions are not identical and  
16 certainly not in this instance. The presented in-vitro conditions do not factor in the  
17 dynamic conditions in living tissue. The surgically treated area would be under  
18 continuous and changing fluids as the organ attempts to bring in the necessary  
19 biocomponents to heal the traumatized tissue. As such, it would not be expected that  
20 the scavenger/formaldehyde ratio would be maintained as it was in the in-vitro state.  
21 It could be speculated that the use of such high loadings of any fluid solubilized  
22 additives would contribute to greater formaldehyde emissions. This can be assumed to  
23 be a consequence of dissolution of the additives resulting in cavities in the polymer  
24 thereby promoting greater surface area for hydrolytic degradation.

25 US patent 5,403,591 concerns the use of cyanoacrylates for treatment of skin  
26 irritations that progress to ulcerations. It would be assumed that these conditions  
27 could be considered wound formations, e.g., see U.S. patent 3,995,641.

28 US patents 5928611, 5981621, 6099807, 6217603 describe methods of inducing  
29 cure of cyanoacrylates by passing the adhesive through a porous applicator tip containing  
30 substances that initiate the polymerization .

31 US patent 6143352 describes methods of altering the pH environment of  
32 cyanoacrylates in order to attenuate or accelerate the rate of hydrolytic degradation by

1 uses of acid and alkaline additives. The formulation of acidic modifiers is problematic as  
2 they tend to inhibit the primary characteristic of these materials, namely, rapid cure on  
3 application to tissue. Data is presented on effects of acidic compositions on previously  
4 cured cyanoacrylates.

5 All of these methods rely on addition of various compositions to effect the  
6 accelerated cure onto the desired substrate. These may induce polymerization by creating  
7 a greater number of initiation sites and or orientation of the monomer for more facile  
8 polymerizations. Other plausible mechanisms can be evoked, but the fact remains that  
9 these materials become a part of the composition. As such these chemical inclusions may  
10 elicit unfavorable reactions in the cured state. In particular, the use of pH-based  
11 accelerators can now contribute to the alkaline hydrolysis of the cyanoacrylate polymer.

12 This is particularly undesirable in medical applications of the cyanoacrylates as  
13 the hydrolysis results in the evolution of formaldehyde. A certain level of formaldehyde  
14 can be tolerated by tissue as it is able to dispose of reasonable concentrations. A solution  
15 to this was to increase the chain length of the cyanoacrylate monomer side group and in  
16 particular that it be alkyl so as to impart hydrophobic character to the resulting polymer.

17 The current and prior art has been able to achieve a synthesis of the octyl  
18 cyanoacrylate at economic levels for applications in the medical field, although  
19 improbable for uses in commercial applications due to reaction yields. A number of  
20 methods have been attempted to improve yields (12). The variables looked at included:  
21 azeotropes, temperature and formaldehyde/cyanoacetate ratio. Other methods have also  
22 included assessment of different catalysts for the condensation reaction. Regardless of the  
23 methods tried, yields become increasingly smaller as the cyanoacetate pendant group  
24 becomes larger.

25 A reported attempt to improve yields is reported in U.S. patent 6,245,933. This  
26 method attempts to avoid yield losses by producing the high yield cyanoacrylate  
27 prepolymers of the lower homologues (methyl & ethyl) and then proceed through a  
28 transesterification with a longer chain alcohol such as the octyl. Three reported examples  
29 with 2-octanol gave yields ranging from 21.8% to 36.2% of crude monomer.

30 From this, it can be seen that high yields are difficult and no doubt subsequent  
31 workup to medically acceptable products result in even lower product output. The  
32 difficulty with methods such as above, is the undesirable side products which are difficult

1 to remove from the main stream. In particular, it is difficult to achieve complete  
2 transesterification reactions on polymeric moieties because of steric obstruction. As a  
3 consequence, purity is compromised as the initial cyanoacrylate prepolymer is not  
4 completely reacted and the lower homologue co-distills with the desired product.

5 Other additives have been used to attenuate various properties, such as modulus  
6 (elasticity), viscosity, thermal resistance, etc. Each and every additive becomes a  
7 substance that must be removed by the surrounding tissue, which generally do not assist  
8 in recovery of the damaged area. In that regard, the addition of these additives must  
9 factor the property improvement against the effect on tissue compatibility.

#### 10 OBJECTS

11 A principal object of the invention is the provision of a new method for curing of  
12 cyanoacrylate adhesives.

13 A further object is the provision of such curing methods that minimize presence  
14 of contaminants and extraneous additives in the resulting cured adhesives with particular  
15 reference to use in medical procedures.

16 Additional objects include:

17 1. Enhancing the cure speed of stabilized cyanoacrylate adhesives by  
18 destabilization treatment that removes stabilizers from them coincidently with their  
19 application onto a substrate.

20 2. The provision of new cyanoacrylate adhesives curing methods that allow for  
21 greater levels of stabilizers therein to be formulated to provide improved shelf life while  
22 not lowering speed of cure upon application.

23 3. Providing for greater latitude of storage of cyanoacrylate adhesives in  
24 packages with less regard for handling thereof.

25 4. Enhancing the cure speed of cyanoacrylate adhesives by a destabilization  
26 treatment that purifies such adhesive coincidently with the application onto a substrate.

27 5. Producing improved cured cyanoacrylate adhesives that exhibit greater  
28 biocompatibility as a consequence of modified polydispersity, especially such adhesives  
29 that exhibit attenuated degradation of the polymer thereby exposing tissue contacting the  
30 adhesive to lower levels of formaldehyde.

6. The provision of improved cyanoacrylate adhesives curing methods that enable the use of difunctional and/or multifunctional cyanoacrylates to optimize properties such as elasticity, porosity, cohesive strength and degradation rates.

7. The provision of improved cyanoacrylate adhesives curing methods that allow for greater degree of freedom in concentration of stabilizers without affecting the final chemical characteristics of such adhesives.

8. The provision of improved cyanoacrylate adhesives curing methods that allow for formulating unadulterated adhesives containing no plasticizers while achieving the elastomeric properties necessary for bonded substrates undergoing multidimensional stresses.

9. The provision of unique devices for use in carrying out the new method of the invention.

Other objects and further scope of applicability of the present invention will become apparent from the detailed descriptions given herein; it should be understood, however, that the detailed descriptions, while indicating preferred embodiments of the invention, are given by way of illustration only, since various changes and modifications within the spirit and scope of the invention will become apparent to those skilled in the art from such descriptions.

## SUMMARY OF THE INVENTION

These objects are accomplished in accordance with the invention by the provision of a method for curing reactive monomeric cyanoacrylate oligomers to undergo macromolecular formations via appropriate destabilization coincidentally with their application to a substrate. Such destabilization chemically and physically removes stabilizing agents so the new method allows for greater levels of stabilizers to be formulated for improved shelf life and not result in slower curing speed upon application to a substrate. Further, this allows for greater latitude of storage in various packages with less regard for product handling.

Cyanoacrylate adhesives that exemplify this invention comprise one or more monomers having the following general structure:



Without encumbering the body of this patent with specific examples of moieties, reference is made to the numerous patents delineating the myriad of groups that can be



1 represented by the moiety designated as R. These are therefore intended to define and be  
2 included by general reference to such prior art and by those knowledgeable thereof.

3 This invention achieves this goal by removing stabilizers in cyanoacrylate  
4 adhesives coincidentally with their application to substrates thereby making the resultant  
5 purified compositions highly susceptible to polymerizations as a result of contact with the  
6 substrates. In one embodiment for effectively using stabilized cyanoacrylate adhesives in  
7 accordance with the invention, they are stored in a device that houses a frangible ampoule  
8 containing such adhesives separate from particulate agent that removes stabilizers from  
9 the adhesive, but within the device. Alternatively, the frangible ampoule may contain the  
10 particulate destabilizing agent separate from the stabilized cyanoacrylate adhesive or both  
11 the stabilized cyanoacrylate adhesive and the particulate destabilizing agent may be  
12 contained in separate ampoules.

13 Such frangible ampoule containing devices may be constructed of any number of  
14 materials that can be shaped or molded or otherwise fabricated to contain the adhesive  
15 and ampoule. Also, it can be made from such materials as to provide a resilient wall  
16 capable of transmitting pressure to the frangible ampoule without loss of its containment  
17 properties. These application devices advantageously further comprise a filtering  
18 component and nozzle for application of the filtered and resulting destabilized adhesive  
19 to the substrate.

20 The application devices preferably are designed to apply the destabilized product  
21 in a continuous manner by appropriate removal of any destabilizing component. An  
22 example of such a device is one that incorporates a removable cartridge of the  
23 destabilizing agent with a reservoir of the appropriate adhesive feeding through the  
24 cartridge.

25 In a preferred embodiment, one of the above described devices containing  
26 isooctyl cyanoacrylate in the crushable ampoule and a weak base anion exchange resin  
27 such as "Ionac AFP329" (Sybron Chemicals, Inc.). The ampoule is crushed and contents  
28 are intermixed so as to optimize maximal contact with the isooctyl cyanoacrylate  
29 monomer for a short period of time. Upon achieving the desired consistency, the contents  
30 are then expressed through the appropriate filter and dispenser tip onto the substrate,  
31 specifically living tissue, mainly human or animal flesh and skin. The application is  
32 accomplished in such fashion as to prevent encapsulation of adhesive by any surrounding



1           The objects are further accomplished in accordance with the invention by the  
2 provision of unique devices for using the method of the invention. Advantageously, such  
3 device is one that (a) delivers the cyanoacrylate adhesive of convenient viscosity by some  
4 degree of partial polymerization and regulated by the interval from the destabilizing  
5 operation to time of application, (b) contains a porous segment for the containment of a  
6 frangible ampoule and other components so as to permit the release of the destabilized  
7 adhesive with no particulate components being released onto the substrate to which it is  
8 applied, (c) delivers the destabilized adhesive through a nozzle to an applicator tip  
9 configured for appropriate application onto the substrate, (d) is configured with the  
10 adhesive in an isolated compartment separate from the destabilizing agent(s), that is able  
11 to release contents into contact with the destabilizing agents, (e) positions the  
12 destabilizing component in a compartment through which the ampoule-released adhesive  
13 passes as it is being delivered to the applicator tip for transfer to the substrate and (f) can  
14 be used to destabilize monomer formulations prior to application to effect the desired  
15 result.

16           A preferred embodiment of a device of the invention comprises a syringe having  
17 an elongated tubular chamber defined by a length of flexible tubing having a proximal  
18 end and a distal end, a dispensing tip on said distal end, means at the proximal end to  
19 apply pressure to said chamber, filter means positioned between the dispensing tip and  
20 the chamber, a frangible ampoule located within the chamber contains stabilized  
21 cyanoacrylate adhesive and particulate destabilizing agent is contained in the chamber  
22 external of the ampoule.

23           In an alternate embodiment of the above described device, the particulate  
24 destabilizing agent is contained in the ampoule and the cyanoacrylate adhesive is  
25 contained in the chamber external of the ampoule.

26           All of the preferred embodiments are meant to further include all of the various  
27 additives useful in the alteration and improvements to cyanoacrylate adhesives as would  
28 make them suitable for placement into the above devices and modifications to these  
29 devices. These can include plasticizers, stabilizers, surface insensitive additives,  
30 tougheners, thickeners, adhesion promoters and other such compositions as would be  
31 evident to those familiar with the cyanoacrylate adhesives art.

1 BRIEF DESCRIPTION OF THE DRAWINGS

2 A more complete understanding of the invention can be obtained by reference to  
3 the accompanying drawings in which:

4 FIG. 1 is a lateral view, partially in section, of a device used in accordance with  
5 the invention for curing stabilized cyanoacrylate adhesives coincidently with their  
6 application to a substrate.

7 FIG. 2 is a lateral view of second embodiment of the dispensing end portion of a  
8 device as illustrated in FIG. 1.

9 FIG. 3 is a lateral view of third embodiment of the dispensing end portion of a  
10 device as illustrated in FIG. 1.

11 FIG. 4 is a lateral view of fourth embodiment of the dispensing end portion of a  
12 device as illustrated in FIG. 1.

13 FIG. 5 is a lateral view, partially in section, of another device used in accordance  
14 with the invention for curing stabilized cyanoacrylate adhesives coincidently with their  
15 application to a substrate.

16 DESCRIPTION OF PREFERRED EMBODIMENTS

17 With reference in detail to the drawings in which generic components are  
18 designated by an arrowhead line and specific components by a plain line, FIG. 1 shows a  
19 first embodiment of a device 2 of the invention for performing the new methods of the  
20 invention comprising syringe 4 having a pliable tubular section 6 partially defined by a  
21 proximal end 8 and a distal end 10 capped with a discharge member 12 defined by a dish  
22 portion 12a and tapered portion 12b plus a funnel 12c structured to operatively engage  
23 the tapered portion 12b.

24 A washer-like member 14 caps the proximal end 8 and admits a plunger 16 with a  
25 distal end 17 that proximally defines a chamber 18. A filter disc 20 fixed in the distal end  
26 10 distally defines the chamber 18 within the tubular section 6.

27 The chamber 18 encloses a frangible ampoule 22 and a quantity of particulate  
28 destabilizing agent 24 as defined herein as an essential material of the invention. The  
29 ampoule is precharged with an adhesive composition 26 comprising cyanoacrylate  
30 adhesive and a stabilizing agent in accordance with the invention thereby being separated  
31 from the particulate destabilizing agent 24 until such time as the ampoule 22 is  
32 fragmented in carrying out the new method of the invention.

1 To accommodate different variations of adhesive application to substrates in  
2 accordance with the invention, the discharge member 12 can be variously structured.  
3 Thus, FIG. 2 illustrates a discharge member 12A similar to member 12, but having a  
4 hemispheric porous filter tip 12d. Also in FIG. 3, the discharge member 12B has a  
5 slotted end 12e to create a ribbon discharge of destabilized adhesive composition from  
6 the device 2 and in FIG.4 the discharge member 12C has a nipple end 12f for drop  
7 dispensing of destabilized adhesive composition.

8 FIG. 5 shows a second embodiment of a device 30 of the invention for performing  
9 the new methods of the invention comprising syringe unit 32, a control valve 34  
10 connected thereto by fluid line 35, a pressure source 36 connected to valve 34 by fluid  
11 line 37 and a suction source 38 connected to valve 34 by fluid line 39. Advantageously,  
12 valve 34 can be a foot operated type so a surgeon using the device 30 will have both  
13 hands free in to apply destabilized adhesive composition to a substrate in accordance with  
14 the invention.

15 Syringe unit 32 has a pliable tubular section 40 partially defined by a proximal  
16 end bulb 42 and a distal end 44 capped with a nozzle 46.

17 A filter disc 48 is fixed in the distal end 44 and distally defines an operation  
18 chamber 50 together with the tubular section 40 and the bulb 42. The chamber 50  
19 encloses a quantity of particulate destabilizing agent 52 as defined herein as essential  
20 material of the invention. In use, the syringe unit 32 will suck a suitable amount of  
21 stabilized cyanoacrylate adhesive into the chamber from a container (not shown) through  
22 nozzle 46 when the valve 34 connects line 35 to the suction source 38. By manipulation  
23 of the pliable tubular section 40, indrawn adhesive (not shown) is mixed briefly with the  
24 destabilizing agent 52. Then, valve 34 is carefully manipulated to intermittently connect  
25 line 35 with the pressure source 36 to force resulting destabilized cyanoacrylate adhesive  
26 out of the chamber 50 via filter 48 and nozzle 46 onto the relevant substrate under the  
27 control, for example, of a surgeon. Following such an operation, the syringe unit 32 will  
28 be disconnected from the line 35 and be discarded, while the remaining units 34, 36 & 38  
29 will be retained for repeated use with new syringe units 32.

30 The following preferred examples further disclose the new method and display its  
31 effectiveness. In these examples, all percentages are by weight unless otherwise  
32 indicated.

1   EXAMPLE 1

2           A quantity of particulate destabilizing agent in the form of suspension type, weak  
3   base anion exchange resin beads is treated with distilled water followed by vacuuming to  
4   0.20 mm Hg at 35-50 degrees centigrade to remove volatiles and moisture.

5           Approximately 1.0 gram of iso-octyl cyanoacrylate monomer is sealed in a  
6   frangible ampoule. Such cyanoacrylate monomer has been stabilized with hydroquinone  
7   at 0.5%. The acid stabilizer, methane sulfonic acid, was introduced previously into the  
8   cyanoacrylate monomer during its synthesis at 0.25%. The cyanoacrylate monomer in the  
9   ampoule and approximately 1.0 gram of the treated anion exchange resin are individually  
10   introduced into a tubular device referred to as a Tandem Dropper supplied by James  
11   Alexander Company of Blairstown, New Jersey, that also provided unsealed ampoules.

12           In order to filter matter dispensed from the dispenser tip of the Tandem Dropper,  
13   it is plugged internally with a small wad of polyester fiber also supplied by James  
14   Alexander Company. The dispenser tip press fits onto the end of the Tandem Dropper to  
15   contain the destabilizing agent and ampoule. The assembled device is activated by  
16   crushing the ampoule. The resultant mixture is then thoroughly mixed by shaking so as to  
17   obtain optimal exposure of monomer to the destabilizing agent. Then, a plurality of  
18   spaced apart drops of the resulting destabilized adhesive are applied to human skin on the  
19   back of a hand and the time for the resulting films to undergo cure to a non-tacky  
20   surface is determined. The destabilized adhesive undergoes cure in 5-15 seconds upon  
21   application to the skin. This contrasts with untreated iso-octyl cyanoacrylate monomer  
22   which shows no sign of cure in 3 minutes.

23   EXAMPLE 2

24           A two milliliter plastic dispensing pipette is cut at the bulb end to permit charging  
25   of destabilizing agent. The pipette is a Number 3 obtained from Poly-Pipets,  
26   Incorporated of Englewood Cliffs, New Jersey. A ¼ inch polyester fibrous plug as  
27   described in Example 1, is inserted down into the narrow tip portion and then 0.5 grams  
28   of anhydrous granular potassium carbonate are charged into the pipette. The plug acts as  
29   a filtration barrier to contain the granular potassium carbonate.

30           The bulb end of the pipette is heat sealed and the resultant device is used to  
31   suction about 1 milliliter of iso-octyl cyanoacrylate monomer for mingling with the  
32   enclosed particulate. The device is positioned with the tip vertically upward and the

1 components are intermingled by successive squeeze and release actions for a short period  
2 of time. Upon satisfactory mixing, the unit is used to apply the resulting destabilized  
3 adhesive onto to skin as thin film portions on the back of a hand. It is determined they  
4 undergo cure in 5-15 seconds. In contrast, untreated iso-octyl cyanoacrylate monomer  
5 exhibits no signs of curing for periods of 3 minutes.

6 This example illustrates the use of multiple applications of the adhesive from a  
7 supply of adhesive and disposable pipettes and foregoes the need for a frangible ampoule  
8 or other adhesive-isolating device.

9 EXAMPLE 3

10 A test was conducted on a wound accidentally caused by a hot surface to the  
11 inside of the left forearm. The wound, approximate dimensions of ¼ inch by 1.5 inches,  
12 had begun to slough off the burned skin exposing the underlying tissue. To evaluate the  
13 protective effect of the destabilized liquid adhesive, the device of Example 2 was used to  
14 apply destabilized iso-octyl cyanoacrylate adhesive. The wound was overlayed with a  
15 thin film and cure took place in the 15-30 second range. The applied and cured  
16 cyanoacrylate adhesive remained well attached for a period of days to the injured skin  
17 while it served to protect the covered wound area from irritation and infection by clothing  
18 or other contact as well as promote the healing process. This contrasted with prior  
19 experiences of similar wounds where the damaged tissue did not heal well due to physical  
20 contact with surrounding irritants such as clothing or other contact surfaces.

21

090322Z JAN 61

# REFERENCES

1. J. A.Collins, et al., ARCH. SURG. Vol 93,428 Sept. 1966
2. F. Leonard, et al., J.A.P.S. Vol. 101617, 1966
3. S. C. Woodward, et al., ANN. SURG. Vol. 162, July 1965.
4. J. J. Cameron, et al., SURGERY, Vol. 58, Aug. 1965.
5. C. H. McKeever, U. S. P. 2912454, Nov. 10, 1950.
6. F. Leonard, et al., J.A.P.S., Vol. 10: 259, 1966
7. R. H. Lehman et al., ARCH. SURG. Vol. 93:441,1966.
8. M. Yonezawa et al., YUKI GOSEI KAGAKU KYOKAISHI, Vol. 25, 1967.
9. F. Leonard, ADHES. BIOL. SYS. 1970.
10. W. R. Vezin et al., J. PHARM. PHARMACOL., Vol. 30, 1978, Suppl..
11. W. R. Vezin et al., J. BIOMED. MAT. RES., Vol. 93, 1980.
12. Yin-Chao Tseng et al., BIOMATERIALS, Vol 11, 1990
13. U.S. Patent 4,057,353
14. U.S. Patent 5,192,536
15. U.S. Patent 3,995,641
16. U.S. Patent 5,254,132
17. U.S. Patent 5,328,687
18. U.S. Patent 5,403,591
19. U.S. Patent 5,928,611
20. U.S. Patent 5,981,621
21. U.S. Patent 6,099,807
22. U.S. Patent 6,217,603
23. U.S. Patent 6,143,352
24. U.S. Patent 6,245,933
25. U.S. Patent 3,667,472